

冷喷涂技术在生物医学领域中的应用及展望

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摘要: 冷喷涂技术 (cold spray technology) 是一类赋予材料表面特殊性能的重要手段。概述了冷喷涂技术在制备温度敏感生物材料加工领域的优势, 并重点综述了利用冷喷涂技术制备的典型生物材料。目前, 冷喷涂沉积永久性植入金属材料, 如 Ti 合金、Fe 基合金、Co-Cr 合金和可降解金属材料 Mg 合金等技术相对成熟。近年来随着冷喷涂技术的发展, 有效解决和拓展了用于医疗器械表面改性的涂层材料体系, 如冷喷涂制备高分子材料超高分子量聚乙烯 (UHMWPE) 涂层, 以及高密度聚乙烯 (HDPE) 和聚醚醚酮 (PEEK) 表面冷喷涂制备生物涂层。最值得关注的冷喷涂或真空冷喷涂技术制备陶瓷涂层, 如羟基磷灰石 (HA)、羟基磷灰石-石墨烯 (HA-graphene) 以及二氧化钛 (TiO₂), 在生物医学领域应用具有突破性进展。同时归纳了冷喷涂技术在生物医学领域的研究现状和问题, 虽然在针对冷喷涂生物涂层的微观结构、力学行为、腐蚀抗力等方面取得了一定成果, 在组织工程、抗菌材料等领域也取得了尝试性突破, 但尚缺乏系统的冷喷涂涂层生物学性能表征, 涂层与细胞/组织相互作用机理还不明确, 相关的临床研究欠缺。最后, 在此基础上, 展望了未来生物材料朝功能化和个性化医疗方向的发展方向。冷喷涂技术在功能化载药涂层的低温制备和个性化医疗器械增材制造等领域将有更大的应用空间, 并给新型生物材料的表面改性带来更多机遇和可能。

关键词: 冷喷涂技术; 生物医疗; 生物材料; 生物学特性

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Applications and Perspectives of Cold Spray Technique in Biomedical Engineering: A Review

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ABSTRACT: High temperature during coating deposition is still the major hurdle that impedes its application for processing temperature-sensitive, oxygen-sensitive or specially designed materials. Cold spray is an emerging coating technique that offers unique and distinctive coating characteristics, and biocompatible metallic materials (Ti- Fe- Co- and Mg-based alloys), polymers (UHMWPE, HDPE, PEEK) and some ceramics (HA, HA-graphene, TiO₂) have been successfully deposited by cold spray processing for tissue engineering and anti-bacterial applications. For cold sprayed biomedical coatings, extensive knowledge has been gained pertaining to fundamental issues about material selection, coating processing, dynamic coating formation, biological performances, and microstructure-property relations. While some of the biomedical coatings are still in the preclinical testing stage. Knowledge on *in vitro* and *in vivo* behaviors of cold sprayed biomedical coatings at different levels is yet insufficient. This review also provides future perspectives of the promising cold spray technique for fabricating advanced biomedical coatings and 3D printing for making biomedical devices.

KEY WORDS: cold spray; biological application; biomaterials; biological properties

随着全球人口老龄化进程的加快,中青年意外创伤的增加,以及人类对自身健康关注度的提高,医疗产业对生物材料的需求量日益增大,未来生物医疗材料的需求将呈现“井喷”势头。针对临床及医疗器械行业对生物材料需求的快速增长,新型生物材料的研发越来越得到重视,材料表面改性技术是目前的研发重点之一,为拓展结构材料在生物医学领域的应用提供技术支撑。表面涂层技术是改善材料表面力学性能和赋予其生物学性能的重要技术手段。其中等离子喷涂是目前唯一被美国食品药品监督管理局授权用于商业化制备移植体表面生物活性涂层的热喷涂技术,但该方法的高温加工特性制约了其在温度敏感生物材料加工领域的应用。因此,冷喷涂技术的发展和开发给生物材料制备带来了更多机遇。

1 热喷涂技术在医疗器械领域的应用

Furlong、Osborn^[1]和 Geesink^[2]首次将表面制备有羟基磷灰石(HA)涂层的生物惰性金属植入手成功应用于临床,标志着表面改性的第二代植入手材料的出现。生物活性涂层的使用可以提高植入手材料的使用性能和使用寿命^[3]。目前,HA涂层被广泛应用于髋骨移植、膝关节移植、踝骨以及肩关节移植等骨科或牙科植入手表面,在硬组织替换和固定方面发挥了很大作用^[4—8]。

等离子喷涂生物活性涂层已经被成功地商业化^[9],但仍存在一些有待解决的问题。Sun^[10]、Heimann^[11]、Tsui^[12—13]、Gadow^[14]、Cheang^[15]等大量学者已经对热喷涂,尤其是等离子制备HA涂

层特性进行了详细描述和系统总结。在利用等离子喷涂制备生物涂层的过程中,材料在经过高温区时不可避免地发生晶粒长大、颗粒尺寸破坏、涂层热应力、相分解以及基体与周围气氛反应等问题^[11]。例如大气等离子喷涂HA后,易形成缺钙HA、氧化钙(CaO)、 α -磷酸三钙(α -TCP)、 β -磷酸三钙(β -TCP)、磷酸四钙(TTCP)、羟基磷灰石(OHA)和无定形磷酸钙(ACP)等相残留。低结晶度HA涂层在生理环境下发生降解和再吸收,易导致涂层与基体的结合强度降低,削弱快速固定效果和植入稳定性。目前,真空等离子弧喷涂与液料等离子可以缓解所制备的涂层含氧量高、低结晶度等问题。相关技术挑战和应用需求对涂层制备技术的发展提出了系列要求,并提供了新的机遇。

2 冷喷涂技术在生物医学领域中的应用现状

20世纪80年代中期,Papyrin等科学家在超音速风洞试验时,发现了超过临界速度的示踪粒子在基体靶材表面沉积的现象,从而发展了冷喷涂技术。冷喷涂技术具有可制备温度敏感材料、增强涂层综合力学性能以及可制备功能载药(生长因子、抗菌剂等)涂层等优势。材料种类直接决定冷喷涂沉积特性及后续性能。

2.1 金属涂层

金属生物材料由于其优异、可靠的力学性能及良好的加工性能,约占整个生物材料市场的40%。

其中, Ti 合金、Fe 基合金以及 Co-Cr 合金已经成为应用最广泛的人造移植金属材料。而医用钛合金体系具有与骨骼相比拟的力学特性, 如更低的弹性模量、更高的疲劳强度和比强度, 已经成为生物医学领域生物金属材料的“金标准”^[16–17]。典型的如 Ti-6Al-4V (TC4)、Ti-3Al-2.5V 等合金, 在临幊上被用作人体胫骨和股骨的替换材料^[18], 但人工髋关节所释放的 V 元素使周围骨组织出现黑化和感染。德国和瑞士先后研制出无 V 的 $\alpha+\beta$ 型第二代低毒性医用钛合金, 如 Ti-5Al-2.5Fe 和 Ti-6Al-7Nb 合金, 但这类合金依然存在与骨骼弹性模量不匹配的应力屏蔽问题, 造成植幊体易松动或失效, 而且 Al 元素的存在对人体存在潜在危害。相比 α 钛合金和 $\alpha+\beta$ 钛合金, β 钛合金的弹性模量低且强度和耐磨性较高, 因此不含 Al、V 的低弹性模量新型医用 β 钛合金 (如 Ti-29Nb-13Ta-4.6Zr、Ti-30Ta、Ti-45Nb 等) 作为第三代医用钛合金成为主要研发方向^[17,19]。

目前, 已有大量工作集中在利用冷喷涂技术制备具有不同微观结构的生物医用 Ti^[20–21]、Ti 合金^[22]以及 Ti 基复合涂层^[23], 并对沉积特性、微观结构、失效行为进行表征。Li 等^[20]发现气体种类和温度显著影响 Ti 涂层的沉积效率和沉积行为。通过控制喷涂参数和热处理工艺, 可调节 Ti 和 Ti-6Al-4V 涂层的孔隙率^[21]。随着冷喷涂技术在增材制造 (3D 打印) 领域的开发应用和拓展, 采用冷喷涂技术进行个性化设计和制备生物医药器件成为可能, 如冷喷涂制备三维结构 Ti 合金半球和嵌有热电偶的 Ti 片等^[24–25]。

相比钛合金, 医用不锈钢具有易加工和低成本等优势, 在硬组织修复和替换方面仍然具有无法替代的作用, 其中, 奥氏体不锈钢 316L、317L 已成为国际公认的外科植幊体首选材料^[26–27], 但是生物不锈钢腐蚀抗力有待提高。Bandar AL-Mangour 等^[28–30]采用冷喷涂制备的医用不锈钢-钴铬合金 (SS316L-L605) 复合涂层与不锈钢涂层相比, 致密性更高且具有更低的腐蚀率, 有望作为一类新型金属生物材料。

医用 Co 合金具有比不锈钢更优异的抗腐蚀性, 是人造关节、口腔材料和心血管支架等的理想替换材料, 但存在 Co、Cr 离子的释放等问题^[31]。这些问题可通过植幊体表面涂层改性处理来应对。Trentin 等在 CoCr 合金基体表面冷喷涂制备生物医用 Ti 合金涂层, 有效降低了金属元素的释放,

并改善了其综合性能^[32]。

Ti 合金、Fe 基合金以及 Co-Cr 合金是永久性植幊体材料, 而 Mg 及其合金是可降解金属生物材料的典型代表, 可利用其降解特性制备非永久性生物移植体, 调控 Mg 合金的降解速率, 在满足医学治疗需要的同时, 可避免患者二次手术带来的痛苦和不必要的经济负担。但是, Mg 合金的腐蚀产物 (如 H₂、Mg²⁺) 以及形成的碱性环境将不同程度地影响人体的代谢功能^[33–34]。目前, Mg 及其合金通常用于接骨板和骨钉等骨固定材料等^[35–37]。但 Mg 是一类高温热敏感且较活泼的金属材料, 冷喷涂技术为这类材料的涂层制备提供了更多可能。Suo 等在 Al、不锈钢基体表面冷喷涂制备 Mg 涂层, 并对沉积行为进行了研究, 结果表明 22~64 μm 粒径范围的 Mg 合金粉末具有最高的沉积效率, 且随着主气温度的提高, 涂层孔隙率随之下降^[38]。进一步研究表明, 基体预热处理可提高基体与 Mg 涂层间的结合强度^[39]。Wang 等在 AZ91 基体表面冷喷涂制备了陶瓷涂层^[40]。

此外, Balla 等研究发现, Ta 合金具有比 Ti 合金更好的生物相容性^[41], 被普遍应用于促进组织生长的多孔支架。Koivuluoto^[42–43]和 Bolelli^[44]等研究者对冷喷涂技术制备 Ta 涂层开展了微观组织结构、腐蚀行为和力学性能的研究, 为新型生物材料的开发和应用奠定了理论基础。

2.2 高分子涂层

高分子移植体具有与天然骨骼接近的力学特性, 可被用作硬组织替换材料。但是在热喷涂制备有机涂层的过程中, 需要严格控制喷涂参数, 避免材料在加热过程中发生非预期转变。

超高分子量聚乙烯 (UHMWPE) 制成的关节臼与金属或陶瓷关节头组成的人工关节, 在过去 50 年已经在临幊中被大量使用^[45–46]。长期临床应用发现, UHMWPE 易发生氧化、老化等, 且产生的磨屑对周围组织的刺激极易引起骨骼炎症和无菌松动^[45–46]。Ravi 等优化了冷喷涂工艺, 可实现在 Al 和聚炳烯 (PP) 基体表面制备厚度为 1~4 mm 的 UHMWPE 和 UHMWPE-Al₂O₃ 复合涂层^[47], 陶瓷颗粒的加入可有效提高 UHMWPE 涂层的致密度、与基体间的结合强度以及耐摩擦性能^[48]。King 等使用冷喷涂技术, 将 Cu 颗粒以高速冲击到高密度

聚乙烯(HDPE)表面实现嵌入式沉积,但是会增加表面粗糙度^[49]。

除了满足基本的力学性能要求外,材料的体内、外生物特性至关重要。一般高分子材料具有一定的生物惰性,很难与宿主骨骼组织形成紧密连接和快速固定。聚醚醚酮(PEEK)在腰间盘移植领域表现出优异的临床效果^[50~51]。目前,已有关于在PEEK基体表面冷喷涂制备Ti^[52]或HA^[53~54]等生物涂层的报道。研究表明,表面经冷喷涂制备HA涂层的PEEK样品,可促进成骨细胞的早期贴附,并能提高细胞活性、ALP酶活性以及钙离子浓度。此外,细胞中的ALP酶、骨唾液蛋白以及相关转录因子-2等作为成骨细胞分化的标志物,其含量也显著提高。采用press-fit方法在兔髂骨中植入冷喷涂HA涂层的PEEK假体,动物体内实验结果证明,冷喷涂制备的生物活性涂层可提高基体材料的生物相容性和骨整合等生物学性能,具有广阔的临床应用前景^[53]。

2.3 陶瓷涂层

与金属和高分子材料相比,陶瓷材料拥有有限的变形能力,目前利用冷喷涂技术制备陶瓷涂层具有一定的挑战性。但随着冷喷涂装备的进一步发展及冷喷涂制备技术的不断成熟,陶瓷涂层的制备和应用会得到进一步拓展^[55]。例如Salim等^[56~57]通过新的合成方法制备了适用于冷喷涂的TiO₂粉末,实现了无添加粘合剂的冷喷涂沉积纯陶瓷颗粒。

临床应用中,Al₂O₃、ZrO₂等惰性生物陶瓷与人体硬组织的结合一般表现为机械锁合,且在体内很难降解,无法被新生组织所替代,主要作为永久替代物应用于临床骨科^[58]。生物活性材料与骨组织具有良好的亲和性,材料与骨组织之间可以形成稳定的结合界面,因此生物活性材料被广泛应用于骨骼修复、口腔治疗以及创口愈合等方面^[59]。

生物活性玻璃是第一代生物活性材料,在过去几十年,出现了大量关于利用热喷涂制备生物活性玻璃涂层的研究报道^[60~62]。但在高温制备过程中,不仅会发生材料成分晶化,使生物活性降低,而且还会引起生物玻璃涂层与基体间的结合强度变差,使涂层易脱落失效^[60,62~63]。利用冷喷涂技术在金属基体表面大面积制备生物活性玻璃涂层,有望从分子水平上刺激特定的细胞反应而加速组织再生,使其降解速度与组织生成速度相匹配,在骨重建过

程中始终能保持足够的力学强度。此外,TCP^[64]、CaSO₄^[65]、CaCO₃^[66]等生物可吸收陶瓷材料同样能随着植入时间的推移而逐渐被吸收^[55,59],相关涂层技术具有一定的应用前景^[60]。

目前,热喷涂技术在制备生物活性陶瓷HA涂层中的应用最成熟,但高温制备过程中所带来的问题依然存在。冷喷涂作为喷涂技术新的发展方向和重要补充,已有研究者尝试在低温或室温下制备HA和HA复合陶瓷涂层,如Noorakma等^[67]采用冷喷涂技术在镁合金AZ51表面制备20~30 μm厚的HA涂层,涂层弹性模量(9GPa)与骨组织接近,并在模拟体液中对镁基体和HA涂层的降解和再生进行了表征。Fujihara等^[68]采用气溶胶沉积技术在Ti基体上成功制备了结合强度大于30 MPa的HA涂层。Liu等^[69~70]采用真空冷喷涂技术在室温下的Ti表面制备了HA和HA-石墨烯复合涂层,结果表明粉末的成分完全保留到涂层中。相对于无涂层的Ti基体,HA和HA-石墨烯复合涂层的微纳米结构更有利于纤连蛋白的快速吸附,并呈现解折叠构象,从而促进成骨细胞的贴附和增殖。

2.4 抗菌涂层

生物材料除了满足必要的力学性能和生物相容性以外,抗菌特性同样备受关注。目前,Sanpo等研究发现冷喷涂制备抗菌的壳聚糖-Cu/Al^[71~72]、HA-Ag/PEEK^[73]等涂层具有较好的生物活性,并对大肠杆菌DH5α具有明显的抑菌效果。进一步研究发现,通过冷喷涂技术在Al6061基体上制备不同比例的ZnO/Ti复合涂层,随着涂层中ZnO含量的增加,涂层对大肠杆菌的灭菌率不断增加,但是涂层表面粘附成骨细胞的活性不断下降^[74]。

TiO₂纳米颗粒在热喷涂过程中,不仅晶粒长大,而且会发生严重的相转变,涂层中残留锐钛矿相比例较低,光催化性能不佳。冷喷涂工艺通过有效地保留锐钛矿相成分,可以获得光催化性能优异的TiO₂涂层,能显著提高涂层的光催化性能^[75]。Yamada^[76]、Yang^[77]、Li^[78]等采用冷喷涂技术制备TiO₂涂层,并对涂层微观组织及光催化特性进行了系统表征。Kilemann等^[79]对Al、Cu、Ti、不锈钢等基体表面的TiO₂颗粒的沉积机理进行了研究,并表征了冷喷涂制备锐钛矿涂层对绿脓杆菌的抗菌作用,在峰值为360 nm的紫外光下照射5 min,细菌的死亡率可达99.99%^[80]。

3 结语与展望

生物材料研究者担负着生物材料体系设计、材料加工以及控制材料生物学响应的责任。现阶段的研究重点主要集中于新型生物材料体系的开发、材料制备技术和装备的拓展、材料-细胞界面机理研究及临床试验等方面。表面工程为生物医疗领域引入了生物材料与组织相互作用的全新概念。冷喷涂医用涂层的相关研究,多聚焦于涂层微观结构、力学行为、腐蚀抗力和基本的生物性能表征等方面,尚缺乏在动物体、器官、细胞、亚细胞,甚至是分子水平对涂层界面特性及涂层与外部生理环境相互作用机理的基础研究。国内外针对冷喷涂生物涂层的应用主要侧重于硬组织替换和抗菌等领域,未来冷喷涂技术在功能化载药涂层低温制备和个性化医疗器械增材制造(3D 打印)等方向有一定的发展空间。随着表面涂层技术的不断发展以及冷喷涂制备技术的逐步完善,冷喷涂生物医用材料将在生物医疗领域得到更多的关注和进一步发展。

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